

# **Respiratory Motion Modelling using cGANs**

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#### BACKGROUND & CONTRIBUTION



**Respiratory motion models** in radiotherapy are considered as one possible approach for **tracking mobile tumours** with the goal of ensuring the best combination of target coverage and dose conformation. We present a motion modelling framework which is:

• patient-specific,

Fig. 1: Schematics of the motion modelling pipeline.

- relying on 2D abdominal ultrasound (US) images as surrogates, and hence on internal motion data,
- capable of predicting **dense volume information** within reasonable computation time.

# Method

**Goal** For every time  $t_j$  we aim to predict a complete MR volume given temporally corresponding abdominal 2D US images.

1) Data acquisition and image registration Simultaneous US/MR imaging is performed based on an interleaved MR acquisition scheme [1] where data and navigator slices were acquired alternatingly. Using deformable image registration [2], 2D deformation fields of the navigator slices are extracted.

(2) Training of the neural network We train a conditional generative adversarial network (cGAN) as proposed in [3] where

### RESULTS

The proposed approach is demonstrated based on 3 hybrid US/MR datasets of 2 healthy volunteers (acquisition duration:  $9.5 \,\mathrm{min}$  each).

**Training details** The datasets were split into  $N_{train} = 480$  training images and  $N_{test} = \{224, 100, 110\}$  test images for datasets  $\{1, 2, 3\}$ , respectively. We applied the U-Net based generator architecture and the convolutional PatchGAN classifier as discriminator.

**Validation** For each consecutive navigator pair of the test set a complete MR volume was reconstructed using the data slices of the training set as possible candidates.

- generator  $G: \{x, z\} \mapsto y$  learns the mapping from US images x and a random noise vector z to the deformation field y, and
- discriminator D aims to classify real and synthesised image pairs.

We introduce gradient information by feeding two consective US images as inputs to the cGAN: given the US images at times  $t_{i-2}$  and  $t_{i-1}$ , we aim to predict the deformation field at  $t_{i+1}$ .

(3) Real-time prediction during dose delivery At time  $t_{j-1}$ , online US images are fed to the trained cGAN generating the deformation field for  $t_{j+1}$ . Following the slice stacking approach in [1], MR data slices acquired in step (1) are grouped into a complete volume predicting the state of the thorax at  $t_j$ .

#### CONCLUSION

A first proof-of-concept study demonstrated the feasibility of the proposed approach. Future work will be devoted towards the development of effective data augmentation strategies and must include a thorough investigation of the robustness of cGANs within the context of motion modelling. **RDF** Reference stacking method using the deformation fields computed on the actually recorded MR navigator slices

 ${\bf GDF}$  Proposed approach based on  ${\bf g}{\bf e}{\bf nerated}$   ${\bf d}{\bf e}{\bf f}{\bf ormation}$   ${\bf f}{\bf i}{\bf e}{\bf l}{\bf d}{\bf s}$ 



Fig. 2: Slice selection illustrated as joint histogram for reference and generated deformation fields, respectively. Left to right: datasets 1 to 3.

## **References** & Acknowledgements

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This work was supported by the Swiss National Science Foundation, SNSF (project number:  $320030_{-}163330/1$ ).



Fig. 3: Qualitative and quantitative results. (a) Sample motion field of dataset 2 with reference (green) and predicted (yellow) deformations, and (b) error distribution of mean deformation field.